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Design and advanced characterization of quercetin-loaded nano-liposomes prepared by high-pressure homogenization

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Nanoliposomes delivering quercetin as senolytic compound: characterization at the nano level and in vitro toxicological effect --Manuscript Draft--

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Abstract:	Quercetin selected as senolytic compound was included into liposomes produced by high pressure homogenization. Particle size, surface charge, and morphology of structures were comprehensively characterized at the nano level by applying traditional and innovative methodologies (i.e. analytical ultracentrifugation, multi-detector asymmetrical-flow field flow fractionation, transmission electron microscopy). The in vitro toxicological effect of loaded liposomes against HCT116 colon cancer cell line was also evaluated. The majority of structures were characterized by oblong shape and dimensions around 30 nm that may have a pivotal role in the physiological outcome. Moreover, the HCT116 cell line was significantly more sensitive to loaded liposomes compared to free quercetin. These results open new frontiers in the design of delivery systems for senolytic components to be included in foods tailored for the ageing population.
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Dear Editor,

We would like to submit the manuscript entitled “*Nanoliposomes delivering quercetin as senolytic compound: characterization at the nano level and in vitro toxicological effect*” by Sofia Melchior, Marta Codrich, Andrea Gorassini, Dora Mehn, Jessica Ponti, Giancarlo Verardo, Gianluca Tell, Luigi Calzolari, and Sonia Calligaris for publication in *Food Chemistry*.

This study is part of a wider research activity dealing with the promotion of the active and healthy ageing of the population, which is a worldwide priority for the scientific community and policymakers. Senolytic therapy is an emerging strategy to promote senescent cell replacement and represents a promising perspective also for designing novel anticancer strategies in combination with current chemotherapy regimens. Different compounds, such as polyphenols, have demonstrated senolytic activity due to their ability to regulate cell senescence, ageing, and longevity. However, the inclusion of these compounds into foods is challenging due to their low water solubility, bioavailability, and stability. The design of carriers for senolytics represents a promising strategy to deliver them in foods up to the target human site. The in-depth characterization of these nanosized structures and their interaction with human cells is pivotal to assess and tailor their functionalities.

The aim of this research was to design and characterize nanoliposomes for the delivery of the senolytic quercetin. To this purpose, high pressure homogenization was used to structure liposomes whose size and shape were investigated by innovative techniques commonly used in nanomedicine field. Senolytic action was investigated by analysing *in vitro* toxicological effect of loaded liposomes against colon cancer cell line. Results confirmed the efficacy of the strategy applied opening new opportunities in food and drug sectors for the promotion of the active and healthy ageing of the population.

Best regards,

27 February 2023

Sofia Melchior

Luigi Calzolari

Highlights

- Liposomes loading senolytic quercetin were produced by high pressure homogenization
- The best-performing treatment for liposome production was 150 MPa for 1 pass
- Liposomes had oblong shape, size around 30 nm and encapsulation efficiency of 42%
- Loaded liposomes exhibited higher senolytic action compared to free quercetin

1 **Nanoliposomes delivering quercetin as senolytic compound: characterization at the nano level**
2 **and *in vitro* toxicological effect**

3

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14 **Abstract**

15 Quercetin selected as senolytic compound was included into liposomes produced by high pressure
16 homogenization. Particle size, surface charge, and morphology of structures were comprehensively
17 characterized at the nano level by applying traditional and innovative methodologies (i.e. analytical
18 ultracentrifugation, multi-detector asymmetrical-flow field flow fractionation, transmission electron
19 microscopy). The *in vitro* toxicological effect of loaded liposomes against HCT116 colon cancer cell
20 line was also evaluated. The majority of structures were characterized by oblong shape and
21 dimensions around 30 nm that may have a pivotal role in the physiological outcome. Moreover, the
22 HCT116 cell line was significantly more sensitive to loaded liposomes compared to free quercetin.
23 These results open new frontiers in the design of delivery systems for senolytic components to be
24 included in foods tailored for the ageing population.

25

26 **Keywords:** senolytics, liposomes, high pressure homogenization, analytical ultracentrifugation, nano
27 delivery system, elderly

28

29 **1 Introduction**

30 Cell senescence is a permanent and irreversible cell cycle arrest that is accompanied by changes in
31 cell morphology and physiology (Kirkland & Tchkonja, 2017). This phenomenon is characterized by
32 different and opposite effects. It is a matter of fact that senescence evolved as a beneficial response
33 to damage promoting wound healing, limiting fibrosis, fighting against cancer, and helping
34 embryonic development. However, the excessive accumulation of senescent cells favours ageing-
35 related diseases as well as other changes associated with ageing and is also an emerging hallmark of
36 cancer chemoresistance (Mária & Ingrid, 2017). Therefore, the design of strategies to selectively
37 reduce senescent cells and improve healthy condition of ageing population is of the utmost
38 importance.

39 Senolytic therapy is an emerging strategy to promote senescent cell replacement, currently in clinical
40 trial for age-related diseases such as sarcopenia, and represents a promising perspective also for
41 designing novel anticancer strategies in combination with current chemotherapy regimens (Chaib,
42 Tchkonja, & Kirkland, 2022). Different compounds have been indicated to exert senolytic activity.
43 Among them, some plant-derived compounds, such as polyphenols, are indicated as promising in
44 regulating cell senescence, ageing, and longevity. As well known, polyphenols represent a large class
45 of natural compounds present in many fruits and vegetables as well as derived products. Typical
46 examples of polyphenols with senolytic activity are quercetin, catechins, cyanidin, curcumin, and
47 resveratrol (Gurău et al., 2018). In particular, quercetin exerts two complementary actions: on one
48 hand, it can promote the death of ageing cells, while on the other hand, it can delay cell senescence
49 and/or promote clearance of senescent cells in healthy tissues (Gurău et al., 2018; Hwang, Tran,
50 Rebuffatti, Li, & Knowlton, 2018).

51 Unfortunately, the simply ingestion of quercetin is not sufficient to guarantee its benefits *in vivo*
52 mainly due to its low bioavailability, *i.e.* the fraction of an ingested compound that eventually ends
53 up in the systemic circulation reaching the site of action in an active form (Chen, Zou, Liu, &
54 McClements, 2016). This is attributed to the physical properties of quercetin, *i.e.* crystallinity and

55 scarce solubility in water (Aditya et al., 2014; Chen et al., 2016; Toniazzo, Peres, Ramos, & Pinho,
56 2017), as well as to its chemical instability being easily degradable and oxidable under moderate
57 alkaline conditions and/or under heat exposure (Aditya et al., 2014).

58 These issues may be overcome by designing proper nanostructured delivery systems, such as:
59 liposomes, emulsions, solid lipid nanoparticles, and lipid nanocarriers in order to encapsulate, protect,
60 and release quercetin at the target site of action (Aditya et al., 2014; Toniazzo et al., 2017). Among
61 them, liposomes – defined as self-assembled vesicles ranging from 10 nm to several micrometres
62 with a phospholipid bilayer structure that separates them from the surrounding aqueous environment
63 have received particular attention (Liu et al., 2020). Several studies have demonstrated the aptitude
64 of liposomes as delivery system for quercetin by guaranteeing both its high stability during storage
65 and bioavailability, while ensuring high encapsulation efficiency (Hao et al., 2017; Toniazzo et al.,
66 2017). The effectiveness of liposomes as delivery systems greatly depends on their dimensions
67 (Haddadzadegan, Dorkoosh, & Bernkop-Schnürch, 2022). It is well known that the particle size of
68 the designed structures is a pivotal factor for their application in food as well as in pharmaceutical
69 products (McClements, 2018). Moreover, considering the physiological behaviour, particle
70 dimensions impact body adsorption, biodistribution in the bloodstream, and excretion behaviour
71 (Gioria et al., 2018). The smaller the particle size, the greater is the surface area exposed to lipase
72 digestion, which may influence the release of the encapsulated bioactive compound and thus its
73 bioaccessibility (Álvarez et al., 2022). Additionally, the smaller the size, the higher is the diffusion
74 coefficient in intestinal mucus especially when the nanocarrier has dimensions below 100-200 nm
75 that is the mesh size of the mucus microstructure (Haddadzadegan et al., 2022). With this regard,
76 attention should be paid to the methodology applied to study the morphology and dimensions of
77 liposomes at the nano-level. No single technique can provide reliable information itself about particle
78 size and distribution, but a combination of instruments, based on different operating principles, is
79 likely to be required for a robust nanometric assessment (Calzolari, Gilliland, & Rossi, 2012). In
80 particular, analytical methods, applied in other fields (*e.g.* medical, environmental), may be adapted

81 to nanostructures intended for food applications. In particular, the usage of nanoparticle tracking
82 analysis, asymmetrical-flow field flow fractionation, or analytical ultracentrifugation together with
83 microscope analysis (*i.e.* transmission electron microscopy) may represent a promising strategy for
84 deep characterization (Gioria et al., 2018).

85 To obtain liposomes, different mechanical (*i.e.* supercritical carbon dioxide, ultrasounds, and high-
86 pressure homogenization) and non-mechanical (*i.e.* reverse-phase evaporation and ethanol injection)
87 interventions can be exploited (Ibišević, Smajlović, & Arsić, 2019; Wagner & Vorauer-Uhl, 2011).
88 Among these, high-pressure homogenization (HPH) guarantees high reproducibility without solvent
89 utilization and allows to generate liposomes with dimensions lower than 100 nm. Moreover,
90 homogenization process could be easily scaled-up since dedicated equipment are already
91 commercially available (Ibišević et al., 2019; Wagner & Vorauer-Uhl, 2011). Besides the process,
92 the choice of the amphiphilic molecule forming liposomes is crucial. Among all, soy lecithin has
93 received great attention due to its abundance as natural source, relatively low production costs
94 compatibility with cell membranes (Quach et al., 2022)

95 Based on these considerations, the aim of the present study was to design nano-liposomes for the
96 delivery of the senolytic quercetin. To this purpose, in the first part of the study, HPH at different
97 processing conditions in terms of homogenization pressure and number of steps was applied to
98 structure lecithin-based liposomes. The resulting systems were then characterized for their size, ζ -
99 potential, and encapsulation efficiency. The best performing process conditions were then used to
100 prepare quercetin loaded nano-liposomes, whose nanostructure was further characterized by applying
101 techniques commonly used in nanomedicine, such as multi-detector asymmetrical-flow field flow
102 fractionation (AF4) and analytical ultracentrifugation (AUC). Finally, the metabolic effect of
103 quercetin-loaded liposomes against colon cancer cells was evaluated.

104

105

106 **2 Materials and methods**

107 *2.1 Materials*

108 Pure soy lecithin was purchased from Carlo Erba Reagenti SpA (Rodano, Milan, Italy); potassium
109 phosphate (K_2HPO_4), quercetin ($\geq 95\%$), kaempferol ($\geq 97\%$; HPLC-DAD Internal Standard; IS),
110 methanol (MeOH) and formic acid for HPLC-MS were purchased from Sigma-Aldrich. HCT-116
111 p53^{+/+} cells were provided by ATCC (Manassas, USA). Dulbecco's modified Eagle's medium, fetal
112 bovine serum, GlutaMAX, penicillin, and streptomycin were provided by EuroClone (Milan, Italy)
113 Milli-Q grade water was produced by the Elgastat UHQ-PS system (ELGA, High Wycombe Bucks,
114 UK).

115

116 *2.2 Liposome preparation*

117 Soy lecithin (10 g/L) added or not with quercetin (0.3 g/L) was dispersed in water and stirred for 1 h
118 at room temperature. The dispersion was then pre-homogenized with a high-speed homogenizer
119 (Ultra-Turrax Homogenizer, IKA, Germany) for 5 minutes at 14,000 rpm. Then, the sample was
120 homogenized using a continuous lab-scale high-pressure homogenizer (Panda Plus 2000; GEA Niro
121 Soavi, Parma, Italy) characterized by two Re + type tungsten carbide homogenization valves and flow
122 rate of 10 L/h. The treatment was conducted at pressures of 50, 100, and 150 MPa for 1 pass and at
123 150 MPa for 3 passes. A sample not subject to HPH treatment was used as control (No HPH). To
124 remove unincorporated material, after HPH, samples were centrifuged (Beckman Coulter, AvantiTM
125 centrifuge, J-25, USA) for 10 minutes at 10,000 $\times g$ and the supernatant containing liposomes was
126 collected for further analysis, while the precipitate were discarded. Samples were prepared with and
127 without quercetin and stored at 4 °C until further analysis.

128

129

130

131

132 2.3 *Analytical determinations*

133 2.3.1 *Turbidity measurement*

134 Turbidity was measured at 660 nm using a UV-Vis spectrophotometer (UV-2501 PC, Shimadzu,
135 Kyoto, Japan) at 25 °C with a 1 cm path-length cuvette.

136

137 2.3.2 *Particle size distribution and ζ -potential*

138 Particle size distribution in batch mode was measured by dynamic light scattering (DLS, Zetasizer
139 NanoZS, Malvern Instruments, Worcestershire, UK). Samples were diluted 1:100 (v/v) with MilliQ
140 water and placed in a cuvette where the scattered laser light (at 173° angle) was analysed.

141 For ζ -potential measurements, samples were placed in a disposable folded capillary cell equipped
142 with two electrodes to assess particle electrophoretic mobility.

143

144 2.3.3 *Encapsulation efficiency by HPLC-ESI-MS-DAD*

145 Encapsulation efficiency (EE, %) was measured by HPLC-ESI-MS-DAD. Samples were diluted 1:20
146 (v/v) with methanol to permit the quercetin release from the liposomes.

147 Each sample (100 μ L) was spiked with 100 μ L of the IS solution (kaempferol, 9.7 μ g/mL in MeOH)
148 and diluted in 1 mL of MeOH/H₂O 70:30 (v/v) with 0.4% of formic acid. The sample was transferred
149 in an autosampler vial for the HPLC-ESI-MS-DAD analysis.

150 Chromatographic analysis was performed with a UHPLC Ultimate 3000 (Thermo Scientific, San
151 Jose, CA, USA) equipped with a column oven and a thermostated autosampler. The chromatographic
152 separation was performed with a column InfinityLab Poroshell 120 EC-C18 (4.6 \times 150 mm, 2.7 μ m;
153 (Agilent Technology, Milan, Italy), thermostated at 30 °C. Elution was carried out at a flow rate of
154 0.3 mL/min, using as mobile phase a mixture of 0.2% formic acid in methanol (A) and 0.2% formic
155 acid in water (B) with the following gradient: 0-13 min 70% A, 15 min 100% A, 26 min 100% A, 28
156 min 70% A, 35 min 70% A. The injection volume was 20 μ L. The HPLC system was coupled with a
157 Ultimate 3000 RS diode array detector (DAD; Thermo Scientific, San Jose, CA, USA) and a Finnigan

158 LXQ linear ion trap mass spectrometer with an electrospray ionization source (ESI-MS; Thermo
159 Scientific, San Jose, CA, USA), in parallel by splitting the mobile phase 1:1. The acquisition was
160 carried out in full scan (m/z 50-1500) and in full scan MS² (m/z 50-600) selecting the precursor ion
161 $[M - H]^-$ at m/z 301.1 for quercetin and at m/z 285.2 for kaempferol (IS). The quantitative analysis
162 was carried out using a diode array detector controlled by Chromeleon software (version 6.80).
163 Spectral data from all peaks were accumulated in the range of 200-400 nm and chromatograms were
164 recorded at 372 nm for both quercetin and kaempferol (IS).

165 A stock solution of quercetin in MeOH/H₂O 70:30 (v/v) with 0.4% of formic acid was serially diluted
166 with the same solvent, with a constant concentration of kaempferol (0.97 μg/mL), to prepare 6-point
167 calibration curve in the range 0.1-3.0 μg/mL. The R² coefficient for the calibration curve was > 0.999.
168 EE (%) was calculated following Eq. 1:

169

$$170 \quad EE (\%) = \frac{\text{encapsulated quercetin } \left(\frac{mg}{mL}\right)}{\text{quercetin in the initial dispersion } \left(\frac{mg}{mL}\right)} \times 100 \quad \text{Eq. 1}$$

171

172 2.3.4 Analytical ultracentrifugation (AUC)

173 AUC analysis was performed using a Beckman Coulter ProteomeLab™ XL-I analytical
174 ultracentrifuge with an 8-hole rotor, collecting interference and absorbance signals simultaneously in
175 the same run. Samples were diluted with water and measurements were conducted at 20 °C at a
176 rotation speed up to 30,000 rpm. Absorbance signals were collected at 250 and 370 nm. The ls-g*(s)
177 distribution model of the SEDFIT software was applied to fit experimental data to calculate
178 sedimentation coefficient distributions. The latter were transformed to hydrodynamic diameter (Dh)
179 using the “transform s distribution to r distribution” option of SEDFIT. Particle viscosity and density
180 were calculated in accordance with the ISO standard n. 18747-2 (ISO, 2019). Samples were diluted
181 in sucrose solutions (5% w/v) and reference cell of the AUC centrepiece was loaded with sucrose
182 solution of the same density.

183 2.3.5 *Multi-detector asymmetrical-flow field flow fractionation (MD-AF4)*

184 The analysis was performed with AF2000 Multiflow FFF (Postnova Analytics GmbH, Landsberg,
185 Germany) equipped with isocratic pumps (Postnova PN1130), degasser (Postnova PN7520), and a
186 manual injector with a 50 µL loop. The system was equipped with three online detectors: multi-angle
187 laser scattering (MALS, Wyatt DAWN HELEOS II MALS detector ($\lambda=661$ nm) equipped with 18
188 detectors at angles from 12.8° to 157.8°; UV-VIS detector (Postnova 3212) set at 250 nm; and DLS
189 equipped with flow-mode cell, detecting in backscattering at 173°. The mobile phase, consisting of
190 phosphate buffer 1 mM (pH 8), was pumped into the channel from opposite ends during injection and
191 focusing, and came out through a 10 kDa cellulose membrane (294 mm x 30 mm, Postnova) at the
192 accumulation wall. When focusing is complete the analyte forms a thin line transverse to the direction
193 of channel and detector flow. Subsequently, the analyte was separated into components based on size
194 as a result of opposing forces of particle diffusion and applied cross flow rate perpendicular to channel
195 or detector flow rate (Parot, Caputo, Mehn, Hackley, & Calzolari, 2020). The optimized method
196 consisted of a focus-injection step for 5 min, followed by elution at detector flow of 0.5 mL/min with
197 an exponentially decaying cross flow from 0.6 to 0 mL/min for 60 min. In this experiment, 50 µL
198 aliquots of sample were used. Online UV-Vis absorbance at 250 nm was utilized for the estimation
199 of mass recovery (R%). The latter was obtained by integrating the area under the UV-Vis peak for
200 each sample eluted with and without the applied cross flow and focusing step using Nova FFF4
201 software (Eq.2).

202

$$203 \quad R (\%) = \frac{\text{UV-Vis area of fractionated sample}}{\text{UV-Vis area of sample without crossflow or focus}} * 100 \quad \text{Eq. 2}$$

204

205 Although different parameters were considered and modified (cross flow, injection time, sample
206 amount and concentration, mobile phase composition and pH) to optimize the process, the maximum
207 recovery (R%) was below 70% that is the minimum limit required by ISO/TS 21362 (ISO, 2018).

208 However, the fractogram and the increase of particle size with the exit time indicated that the applied
209 method was satisfactory to achieve the separation of liposomes with different sizes while
210 guaranteeing high reproducibility (Iavicoli et al., 2015).

211 The geometric diameter (D_g) was computed through the Wyatt ASTRA software by using the Zimm
212 model, typically applied for small particles, and the sphere model obtaining R^2 higher than 0.7 and
213 0.9, respectively. The hydrodynamic diameter (D_h) was obtained by analysing DLS flow data with
214 the Zetasizer software. The shape factor was calculated as the ratio between D_g and D_h . For each
215 sample, the analysis was performed in triplicate.

216

217 2.3.6 *Transmission electron microscope (TEM)*

218 Shape and size of liposomes were analysed by direct visualization using Cryo-TEM technique
219 (Burrows and Penn, 2013). Briefly, 4 μ L of liposomes stock suspension were applied to 200 mesh
220 copper Lacey Carbon Film grid (Agar Scientific, UK) pre-treated by Leica EM ACE200 glow
221 discharge (10mA, 30s; Leica, Italy). Excess material was blotted away by filter paper and sample
222 vitrification was done using Leica EM GP (Leica, Italy) equipment. Sample was immediately
223 analysed by TEM at 120kV (JEOL-JEM 2100, JEOL, Italy) equipped with Gatan cryo transfer holder
224 626 (Gatan, USA).

225

226 2.4 *Cell cultures*

227 HCT-116 p53^{+/+} (ATCC) cells were grown in Dulbecco's modified Eagle's medium supplemented
228 with 10% fetal bovine serum, 2 mM GlutaMAX and 100 U/mL penicillin and 10 μ g/mL streptomycin.

229

230 2.4.1 *Cell Metabolic Assay*

231 Cell line viability was measured using the colorimetric method CellTiter 96[®] AQueous One Solution
232 Proliferation assay (MTS) (Promega, Madison, WI, USA) according to the manufacturer's protocol.
233 In detail, 5000 cells were plated on transparent 96-well plates. The day after, cells were treated with

234 empty liposomes, quercetin-loaded liposomes, or quercetin alone, and the viability of the cells was
235 measured by recording the absorbance at 490 nm with a plate reader (Enspire PerkinElmer, Waltham,
236 MA, USA).

237

238 2.5 *Statistical analysis*

239 All determinations were expressed as the mean \pm standard deviation (SD) of at least three
240 measurements. Analysis of variance (ANOVA) and t-test were performed by using R v. 4.1.1 for
241 Windows (The R foundation for statistical computing). A Tukey's *post-hoc* test was used to assess
242 differences between means ($p < 0.05$).

243

244 **3 Results and discussion**

245 3.1 *Definition of the best processing condition for liposome preparation*

246 The effect of high-pressure homogenization (HPH) conditions (pressure and number of passes) on
247 liposome formation was firstly evaluated. Table 1 shows turbidity, measured at 660 nm, particle size
248 distribution, ζ -potential, and encapsulation efficiency (EE) of liposomes with and without quercetin.
249 The turbidity of liposomes without quercetin decreased as the homogenization pressure increased.
250 However, by increasing the number of passes at 150 MPa further increased the turbidity values. Since
251 turbidity is associated to the size and distribution of particles, particle size distribution was also
252 analysed (Figure S 1). All samples were polydisperse as indicated by PDI values higher than 0.2. The
253 control sample presented the highest Z-average (Z-ave) and PDI above 0.5 indicating very broad size
254 distribution (Figure S 1a). The application of HPH induced the formation of liposomes with less
255 polydisperse distributions that decreased as a function of pressure increase and as a result of increased
256 intensity of shear forces suffered by the sample during the passage through the homogenization valve.
257 Sample prepared at 150 MPa for 1 pass had the lowest PDI (0.282 ± 0.007) and Z-ave of 69.3 ± 0.8
258 nm. These results were in agreement with previous studies that reported the dependence of particle
259 size reduction on HPH pressure increase (Barnadas-Rodríguez & Sabés, 2001). Although Z-ave was

260 the lowest, by further increase HPH intensity (150 MPa for 3 passes) PDI of liposomes significantly
261 ($p<0.05$) increased, indicating the reduction of size homogeneity probably due to aggregation and/or
262 destabilization of particles upon treatment (Ibišević et al., 2019).

263 Similar results were observed for quercetin-loaded liposomes. Overall, compared with unloaded
264 samples, liposomes with quercetin were characterized by higher turbidity and particle dimensions
265 (Figure S 1) probably because the bioactive compound affected liposome characteristics. This
266 phenomenon was also observed by Toniazzo *et al.* (2017) that reported average particle size of
267 quercetin loaded liposomes higher than that of unloaded ones. Similarly, Gibis, Ruedt, & Weiss
268 (2016) observed the same behaviour when grape-seed polyphenols were incorporated into liposomes.
269 The increase of particle size of loaded structures may be attributed to the location of quercetin closer
270 to the centre of the lipid bilayer. This may adversely affect the colloidal stability of liposomes by
271 reducing the surface exposure of the phosphate head groups leading to the system destabilization
272 (Malekar, Sarode, Bach, & Worthen, 2016).

273 ζ -potential (Table 1) become more negative by increasing pressure up to 150 MPa, while a slight
274 increase was observed for the sample produced at 150 MPa for 3 passes probably due to system
275 destabilization, as confirmed by previous data. The progressive tendency of ζ -potential to get close
276 to -30 mV indicated that the physical stability of liposomes increased with pressure (Madureira et al.,
277 2015). Interestingly, the effect of treatment was less pronounced in loaded liposomes probably due
278 to the location of quercetin in the middle of lecithin bilayer, which leads to reduced exposure of
279 phosphate groups (Malekar et al., 2016), as previously speculated.

280 Finally, encapsulation efficiency (EE) (Table 1) ranged from 31% to 42%. These results are in
281 agreement with those by other authors reporting EE between 32% and 50% in the case of liposomes
282 containing black carrot extract produced by HPH (Guldiken, Gibis, Boyacioglu, Capanoglu, & Weiss,
283 2017). As expected, and in agreement with previous observation, EE increased as a function of
284 pressure increase, achieving the highest value of $42.11 \pm 4.08\%$ at 150 MPa, while the lowest one
285 was obtained at 150 MPa for 3 passes. Beside the process conditions, EE results also depend on the

286 solubility of quercetin in the lecithin bilayer (Guldiken et al., 2017). Complete liposome
287 encapsulation may be achieved only if the encapsulated material is soluble in the liposome membrane
288 (Bryła, Lewandowicz, & Juzwa, 2015), as observed considering the delivery of hibiscus (61–72%),
289 elderberry (25%), and grape seed (88%) (Bryła et al., 2015; Gibis et al., 2016; Gibis, Zeeb, & Weiss,
290 2014).

291 Based on the acquired results, liposomes obtained at 150 MPa for 1 pass were selected as the best
292 delivery system due to their smaller particle size, good physical stability, inferred from ζ -potential
293 value, and the highest EE as compared with the other samples.

294

295 3.2 *Nanostructure of liposomes*

296 Quercetin-loaded and unloaded liposomes, produced by applying the best performing condition (150
297 MPa for 1 pass), were in-depth characterized for their size. As previously discussed, DLS in batch
298 mode is not always appropriate to measure the dimensions of nanoparticles (Caputo, Arnould, et al.,
299 2019; Caputo, Clogston, Calzolari, Rösslein, & Prina-Mello, 2019; Gioria et al., 2018; Mehn, Caputo,
300 et al., 2017). Thus, analytical ultracentrifugation (AUC) and asymmetric flow field flow fractionation
301 (AF4) were performed. These techniques have been recently proposed in the nanomedicine field to
302 characterize the size of nanostructures, such as liposomes (Iavicoli et al., 2015; Mehn, Capomaccio,
303 Gioria, Gilliland, & Calzolari, 2020; Mehn, Iavicoli, et al., 2017) and lipid nanoparticles (Caputo,
304 Arnould, et al., 2019).

305 AUC monitors the sedimentation profile of particles in real time and, by the application of a suitable
306 model, allows the calculation of the particle diameter (Planken & Cölfen, 2010) if density of the
307 particles is known. Figure 1 reports the size distribution of liposomes, with or without quercetin,
308 acquired at 250 nm. Free liposomes were characterized by an almost monodisperse distribution with
309 a mean diameter around 30 nm. The same particle family was detected also in loaded samples, but in
310 this case the distribution was broader. An additional peak was observed at 52 nm, while larger
311 particles were depicted to a lesser extent. Loaded samples were also analysed at 370 nm, which is the

312 quercetin peak of absorbance, to evaluate the role of the bioactive molecule on liposome structure.
313 As previously observed, the addition of quercetin probably interfered with liposome formation
314 resulting in structures with higher dimensions (around 65 nm) as compared with the profile acquired
315 at 250 nm and attributable only to lecithin.

316 Overall, AUC results highlighted that the size of the majority of particles was almost three times
317 lower than that measured by DLS in batch mode, which were: 99.3 ± 4.5 nm and 110.6 ± 2.5 nm for
318 unloaded and loaded samples, respectively (Figure S 1d). Such findings also point out the limitations
319 of DLS in batch mode, such as its low resolution in complex media and in presence of multiple
320 populations in similar size ranges, confirming the necessity to apply other techniques, such as AUC,
321 when dealing with particle size characterization in the nano scale (Caputo, Arnould, et al., 2019;
322 Gioria et al., 2018).

323 AUC results were confirmed by data obtained by AF4. The latter is a high-resolution sizing technique
324 based on the introduction of a fractionation step that separates particles based on their size prior to
325 the detection, without affecting their “soft” structure. Moreover, AF4 offers the possibility to combine
326 multiple on-line detectors, overcoming the limitations of traditional batch mode DLS, while ensuring
327 high size measurement (Caputo, Arnould, et al., 2019; Parot et al., 2020). Results acquired by AF4
328 using different detectors (*i.e.* UV-Vis, MALS, and DLS) are reported in Figure 2.

329 Observing the UV-Vis profile of unloaded samples (black line in Figure 2a), two main peaks were
330 detected. The first one (8.6 min) showed the highest intensity, while the second one (between 25 and
331 60 min) was less intense and broader. UV-Vis data were combined with those acquired by MALS
332 detector, in order to obtain information about the geometric diameter (D_g) of liposomes and their
333 abundance. Three main particle families having different dimensions were observed. Two of them
334 (green and red lines in Figure 2a) were detected in correspondence with the highest UV-Vis intensity,
335 indicating that the majority of liposomes belong to these particle families with D_g ranging from 42
336 to 65 nm. The third particle family (violet line in Figure 2a) appeared with the second UV-Vis peak,
337 indicating the presence of liposomes with dimensions higher than 80 nm. Loaded liposomes (Figure

338 2b) showed the same behaviour but, in this case, the dimensions of the smallest particles were slightly
339 higher (50 - 71 nm).

340 The availability of the online Dg obtained by MALS, as well as the hydrodynamic diameter (Dh)
341 detected with DLS in flow mode (yellow dots in Figure 2), allows to gain information on the
342 morphology of particles by calculating the shape factor (ρ). It is interesting to note that the majority
343 of liposomes, independently on the addition of quercetin, presented Dg higher than Dh, resulting in
344 $\rho > 1$, which is typical of oblong nanoparticles (*i.e.* nanorods, nanotubes, or nanofibers) (Iavicoli et
345 al., 2015). The applied process conditions (150 MPa for 1 pass) probably favoured the production of
346 spherical uniform liposomes. However, this heterogeneity in particle shape could have a favourable
347 effect not only for the liposome applications in food preparation, but also considering the potential
348 biological fate of encapsulated quercetin (Zhou & McClements, 2022). As observed for drug delivery,
349 rod-shaped particles or non-spherical ones are taken up and transported across the intestinal cells to
350 a greater extent compared to those with spherical shape (Banerjee, Qi, Gogoi, Wong, & Mitragotri,
351 2016).

352 Shape and size data were corroborated by direct visualization of liposomes with Cryo-TEM (Figure
353 3). Micrographs highlighted the presence of structures with heterogeneous dimensions in the same
354 range previously detected by AUC (Figure 1) and AF4 (Figure 2). Moreover, spherical and oblong
355 liposomes were observed, confirming previous speculations. In this regard, it is interesting to note
356 that the treatment applied was able to generate liposomes with different structures (*i.e.* unilamellar,
357 multilamellar, and multivesicular vesicles), that may improve the stability and delay sustained-release
358 of quercetin (Liu et al., 2020).

359

360 3.3 *Quercetin-loaded liposomes are able to enter colon cancer cells efficiently.*

361 To test the effects of quercetin-loaded liposomes *in vitro*, we took advantages of a colon cancer cell
362 line (HCT-116 p53^{+/+} cells), that is wild-type for TP53 gene expression (Bunz et al., 1998).
363 Experimentally, HCT-116 p53^{+/+} cells were treated with increasing concentrations of quercetin-

364 loaded liposomes or free quercetin for 48 h. The control cells were treated with unloaded liposomes
365 and the vehicle DMSO, respectively. Then, we evaluated the metabolic activity of viable cells by
366 using the MTS assay (Figure 4). We observed that HCT-116 p53^{+/+} cell line was significantly more
367 sensitive to quercetin-loaded liposomes, at the doses of 50 μ M and 100 μ M, than free quercetin. We
368 did not find a statistically significant difference between quercetin-loaded liposomes and free
369 quercetin at lower doses, even though a differential effect can be observed. Notably, at 100 μ M no
370 differences were detected between loaded and unloaded liposomes. This result could be attributed to
371 soy lecithin that is involved in several metabolic and intracellular process, such as necrosis and
372 apoptosis. Previous studies have also demonstrated that surface active molecules (*i.e.* lecithin, bile
373 salts, phospholipids as well as anionic, cationic, and nonionic surfactants) may reduce the viability of
374 model colon cancer cells through several mechanisms including the disruption of cell membranes,
375 the modification of active transporters, and the competition with the cells for the surface of the cell
376 culture plates, thereby promoting cell detachment (Li, Le Maux, Xiao, & McClements, 2009; Robert,
377 Couédelo, Vaysse, & Michalski, 2020).

378 However, treatment with the quercetin-loaded liposomes significantly reduced the metabolic activity
379 of the HCT-116 p53^{+/+} cell line with respect to unloaded liposomes at the doses of 50 μ M.

380 In conclusion, colon cancer cells are significantly more sensitive to quercetin-loaded liposomes
381 compared to free quercetin and unloaded liposomes, meaning that quercetin-loaded liposomes are
382 able to enter the cell in an efficient manner.

383

384 **4 Conclusions**

385 Lecithin-based liposomes produced by HPH resulted good candidates for the delivering of the
386 senolytic compound quercetin. The process conducted at 150 MPa for 1 pass results the most
387 profitable being able to form liposomes with high encapsulation efficiency and nano-dimensions
388 (around 30 nm), as demonstrated by the use of advances analytical techniques, such as AUC and AF4,
389 scarcely applied in the food sector. The quercetin loaded nano-sized liposomes showed better capacity

390 to act as senolytic agent in colon cancer cells in comparison free quercetin and unloaded systems.
391 These findings suggest that the delivery of quercetin within liposomes may represent a promising
392 strategy to improve its senolytic activity opening new opportunities in food and drug sectors.

393

394 **Declaration of Competing Interest**

395 The authors declare that they have no known competing financial interests or personal relationships
396 that could have appeared to influence the work reported in this paper.

397

398 **Author's contributions**

399 S.M.: Formal analysis, Investigation, Data curation, Methodology, Writing original draft,
400 Visualization, Writing - Review & Editing; M.C.: Formal analysis, Investigation, Data curation,
401 Writing original draft, Visualization, Writing - Review & Editing; A.G.: Formal analysis,
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403 Editing; D.M.: Formal analysis, Investigation, Methodology, Visualization, Writing - Review &
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407 Supervision; L.C.: Visualization, Supervision, Resources, Writing - Review & Editing S.C.:
408 Supervision, Visualization, Resources, Writing original draft, Writing - Review & Editing.

409

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415

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524 **Figure captions**

525 **Figure 1** Size distribution measured with AUC of liposomes (black line) and liposomes with
526 quercetin (dotted black line) calculated from the absorption-based measurement at 250 nm. Grey line
527 indicates the distribution of loaded liposomes with adsorption-based measurement at 370 nm.

528

529 **Figure 2** MD-AF4 fractograms of liposomes (a) and loaded liposomes with quercetin (b). Black line:
530 UV-Vis linear response at 250 nm; yellow dots: hydrodynamic diameter obtained by DLS in flow
531 mode; green and red dots: geometric diameter of the first two size populations detected by MALS
532 and elaborated by the Zimm model; violet dots: geometric diameter of the third size population
533 detected by MALS and calculated by the Sphere model. The maximum recovery for both loaded and
534 unloaded liposomes is reported in the insight.

535

536 **Figure 3** cryo-TEM micrographs of liposomes.

537

538 **Figure 4** Quercetin-loaded liposomes affect cell metabolism in a colon cancer cells model. MTS
539 assay on HCT-116 p53^{+/+} cells. Cells were treated with increasing amounts of free quercetin (free Q),
540 unloaded liposomes (L), or quercetin-loaded liposomes (QL) at the indicated concentrations for 48 h.
541 In graph, the percentage of metabolic activity relative to untreated cells (for L- and QL-treated cells)
542 and to DMSO-treated cells (for free Q-treated cells), both arbitrary set to 100%, is represented. Values
543 are mean \pm SD (n=3).

544

545 **Figure S 1** Particle size distribution as a function of intensity (%) of liposomes (solid line) and
546 liposomes containing quercetin (dotted line) obtained by high-speed homogenizer (a), and HPH at 50
547 (b), 100 (c), 150 (d) MPa for 1 pass and 150 MPa for 3 passes (e).

Table 1 Absorbance at 660 nm, ζ -potential, Z average (Z-ave), polydispersity index (PDI) and encapsulation efficiency (EE) of liposomes with and without quercetin produced by high-speed homogenization (control) and high-pressure homogenization (HPH) at different conditions.

Presence of quercetin	Homogenization pressure	Number of passes	Turbidity (-)	Z-ave (nm)	PDI (-)	ζ -potential (mV)	EE (%)
without quercetin	0 (control)	-	0.405 ± 0.003 ^{a,B}	163.8 ± 2.4 ^{a,B}	0.522 ± 0.008 ^{a,A}	-20.20 ± 0.79 ^{a,B}	
	50 MPa	1	0.122 ± 0.004 ^{b,B}	96.1 ± 1.5 ^{b,B}	0.349 ± 0.035 ^{b,B}	-21.87 ± 1.11 ^{bc,A}	
	100 MPa	1	0.055 ± 0.001 ^{d,B}	73.4 ± 1.4 ^{c,B}	0.292 ± 0.019 ^{cd,B}	-20.73 ± 0.68 ^{ab,A}	
	150 MPa	1	0.047 ± 0.001 ^{e,B}	69.3 ± 0.8 ^{d,B}	0.282 ± 0.007 ^{d,B}	-23.72 ± 0.62 ^{d,B}	
	150 MPa	3	0.062 ± 0.001 ^{c,A}	53.7 ± 1.5 ^{e,B}	0.331 ± 0.035 ^{bc,B}	-22.08 ± 0.45 ^{c,B}	
with quercetin	0 (control)	-	0.720 ± 0.001 ^{a,A}	267.0 ± 10.2 ^{a,A}	0.529 ± 0.018 ^{a,A}	-18.50 ± 1.21 ^{a,A}	32.93 ± 0.12 ^b
	50 MPa	1	0.282 ± 0.062 ^{b,A}	117.0 ± 4.4 ^{b,A}	0.437 ± 0.027 ^{b,A}	-21.70 ± 1.10 ^{b,A}	37.04 ± 0.13 ^{ab}
	100 MPa	1	0.109 ± 0.028 ^{c,A}	88.4 ± 6.3 ^{c,A}	0.464 ± 0.049 ^{b,A}	-21.58 ± 1.33 ^{b,A}	34.13 ± 0.24 ^b
	150 MPa	1	0.085 ± 0.001 ^{c,A}	92.6 ± 1.2 ^{c,A}	0.323 ± 0.009 ^{c,A}	-21.94 ± 1.39 ^{b,A}	42.11 ± 4.08 ^a
	150 MPa	3	0.056 ± 0.000 ^{c,B}	72.0 ± 2.9 ^{d,A}	0.550 ± 0.019 ^{a,A}	-20.04 ± 0.81 ^{ab,A}	31.19 ± 0.06 ^b

Mean ± standard deviation (n>2). ^{a-c}: means indicated a significant difference ($p<0.05$) among different treatments; ^{A-B}: means indicated a significant difference ($p<0.05$) among loaded and unloaded liposomes.

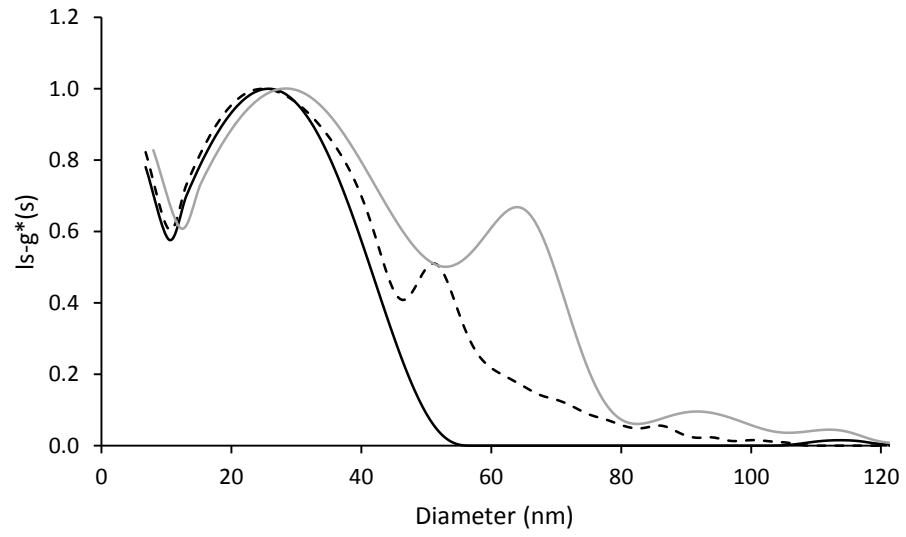


Figure 1

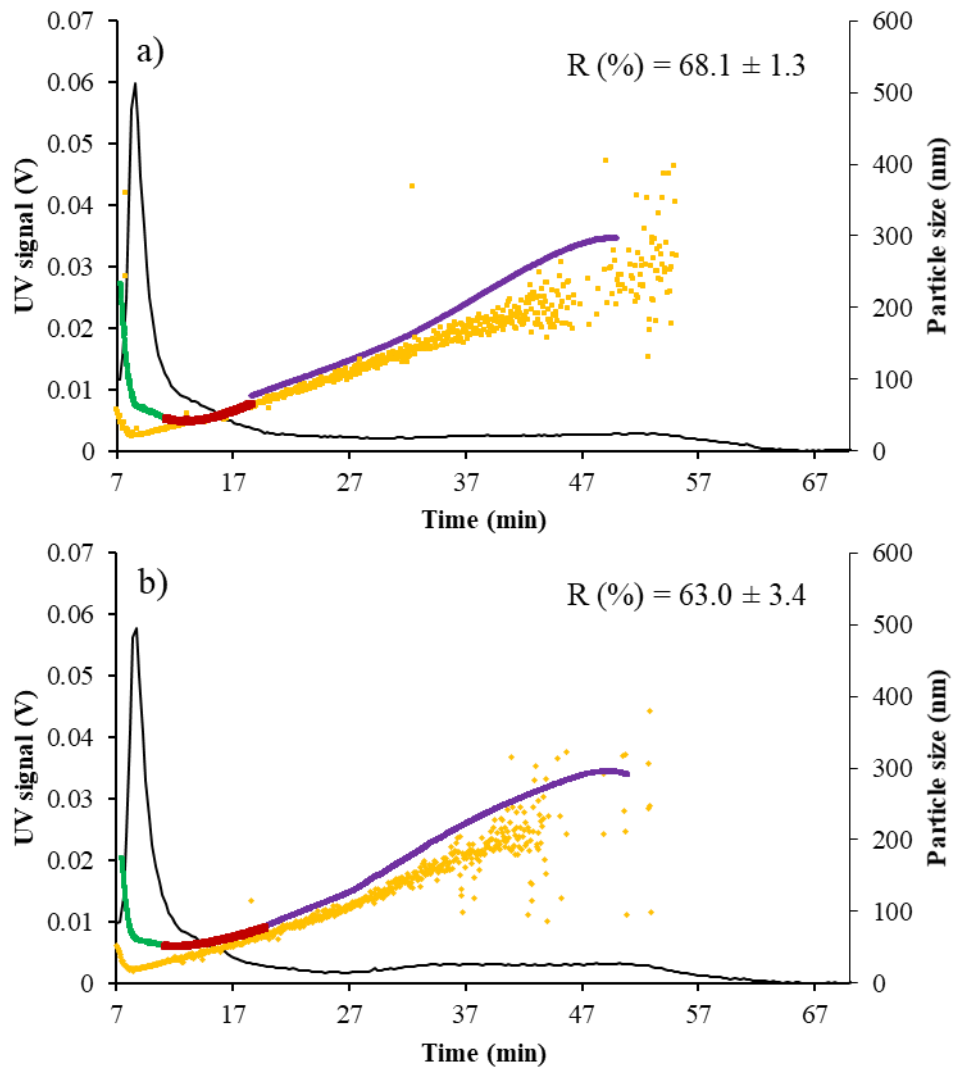


Figure 2

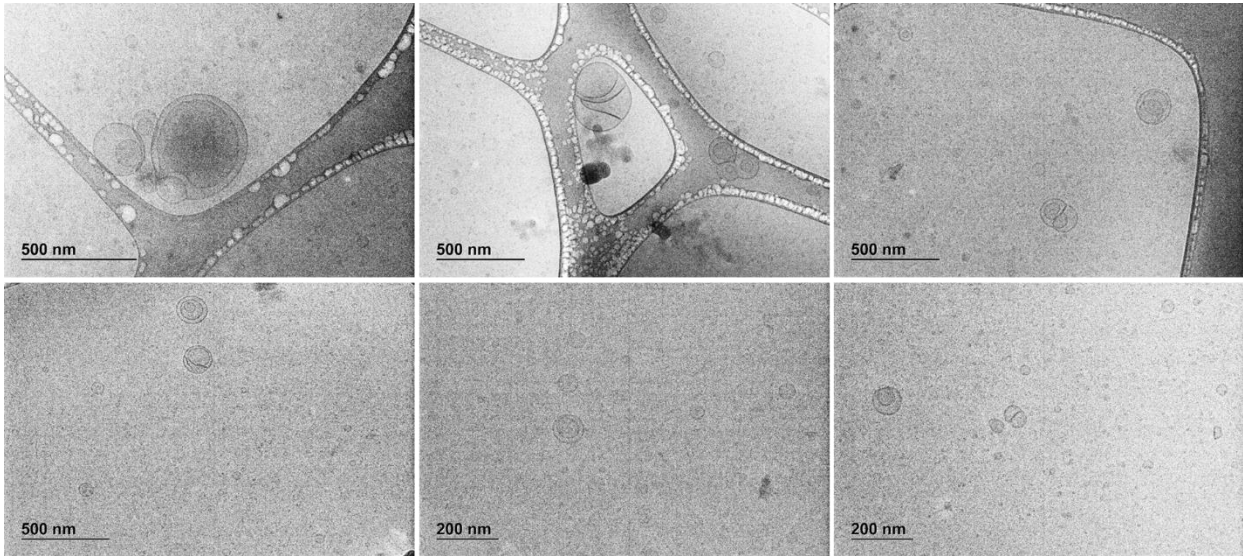


Figure 3

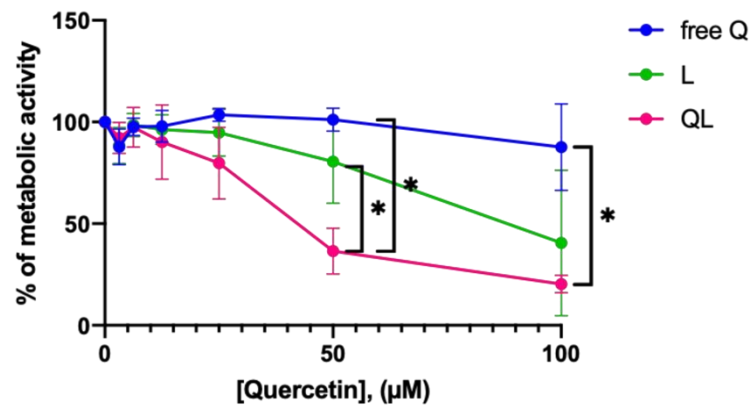


Figure 4

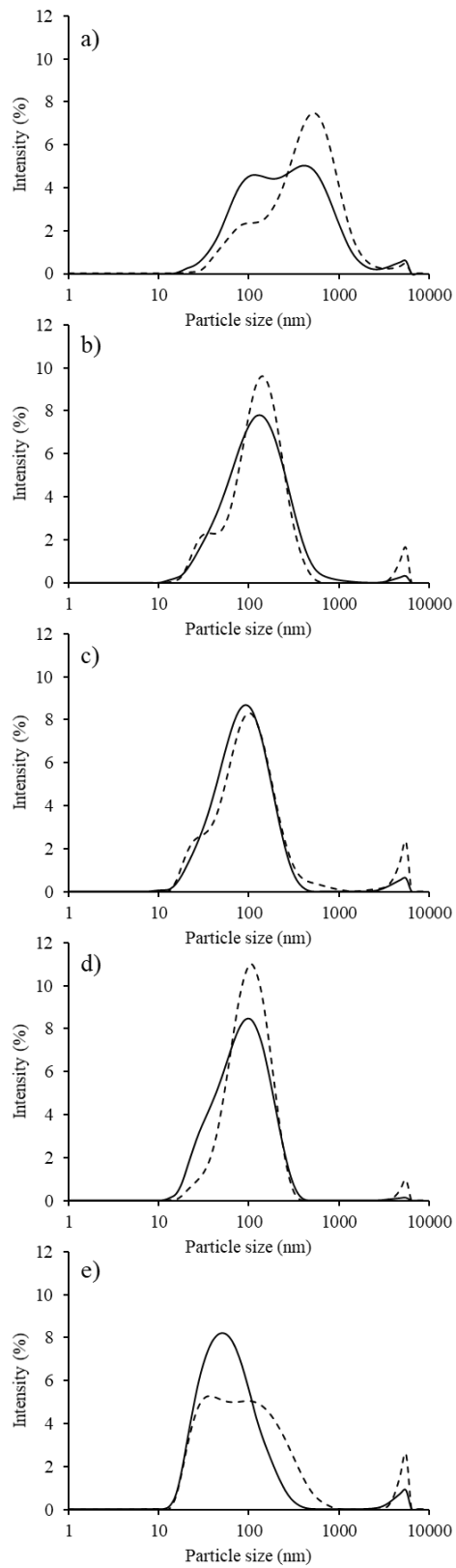
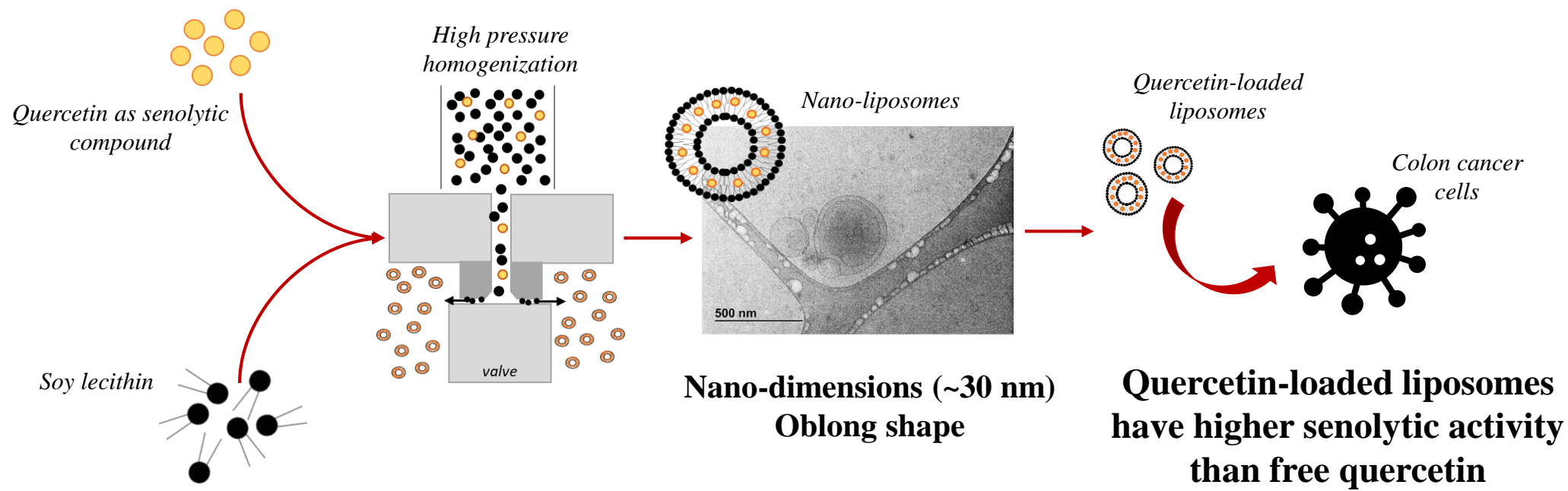


Figure S 1



Author Conflict of Interest Declaration

We wish to confirm that there are no known conflicts of interest associated with this publication and there has been no significant financial support for this work that could have influenced its outcome.

We confirm that the manuscript has been read and approved by all named authors and that there are no other persons who satisfied the criteria for authorship but are not listed. We further confirm that the order of authors listed in the manuscript has been approved by all of us.

We confirm that we have given due consideration to the protection of intellectual property associated with this work and that there are no impediments to publication, including the timing of publication, with respect to intellectual property. In so doing we confirm that we have followed the regulations of our institutions concerning intellectual property.

We further confirm that any aspect of the work covered in this manuscript that has involved experimental animals has been conducted with the ethical approval of all relevant bodies and that such approvals are acknowledged within the manuscript.

We understand that the Corresponding Authors are the sole contact for the Editorial process (including Editorial Manager and direct communications with the office). They are responsible for communicating with the other authors about progress, submissions of revisions and final approval of proofs. We confirm that we have provided a current, correct email address which is accessible by the Corresponding Authors (sofia.melchior@uniud.it and luigi.calzolari@ec.europa.eu).

Udine, 27 February 2023

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